

# Refractive index sensor based on the micromachined side-hole optical fibre

Rafał Kosturek<sup>1\*</sup>, Michał Dudek<sup>1</sup>, Mariusz Zdanowicz<sup>2</sup>, Leszek R. Jaroszewicz<sup>1</sup>, Tomasz Osuch<sup>2,3</sup>

<sup>1</sup>Institute of Applied Physics, Military University of Technology, ul. gen. Sylwestra Kaliskiego 2, 00-908 Warsaw, Poland

<sup>2</sup>National Institute of Telecommunications, ul. Szachowa 1, 04-894 Warsaw, Poland

<sup>3</sup>Faculty of Electronics and Information Technology, Institute of Electronic Systems, Warsaw University of Technology, ul. Nowowiejska 15/19, 00-665 Warsaw, Poland

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## Abstract

An intensity-based refractive index (RI) sensor using a laser micromachined side-hole optical fibre (S-H OF) is presented in this paper. To achieve this, a microcavity was cut into a side surface of the S-H OF, providing access to one of the air holes within its structure. The geometrically modified fibre was then connected at both ends to a single-mode fibre for structure investigation in a system containing a supercontinuum laser and an optical signal analyser. In the next step, an immersion liquid was applied to a microcavity for RI values ranging from 1.30 to 1.57 in increments of 0.02. Power loss measurements were conducted for each RI value. Based on the obtained results, it can be concluded that an RI sensor has been successfully developed, which holds potential applications in biochemistry.

## 1. Introduction

In the last decade, there has been a remarkable progress in the field of fibre optic sensor (FOS) technology. FOSs play a significant role due to their numerous advantages over traditional sensors [1, 2]. These include immunity to electromagnetic interference, high resolution and accuracy, compact size, suitability for long-distance applications, and resilience to high temperatures [3, 4]. Many experimental FOS setups have already found their way into practical applications across various domains. The increasing demand for special fibres with unique characteristics has pushed academic and industrial environments to develop technologies enabling the creation of sophisticated FOS systems [5–7]. The main challenge in manufacturing the FOS is to achieve the ability to interact with the parameters of the light passing through its core which is typically surrounded by cladding. It is necessary to modify its geometry to make the fibre sensitive to changes in the environmental conditions in which it is placed. Modification of the structure can occur through intervention in the facet

or side-surface of the fibre [8, 9]. Methods such as D-shape fibre formation [10, 11], chemical etching [12, 13], polishing [14, 15], tapering [16, 17], and laser micromachining [18–20] can be employed for this purpose. Among the mentioned techniques, laser micromachining is one of the most precise methods for shaping the surface of an optical fibre, commonly used to create cavity structures. This technological procedure allows access to the fibre core, which enables the interaction of the light passing through it with the surrounding medium. This sensor allows for the measurement of specific physical parameters by detecting changes in the external refractive index (RI) [21, 22]. The cut length of the cavity plays a crucial role in determining optical losses, the most significant parameter in these sensors. These losses can be easily measured and translated into precise changes in the cavity environment, essentially functioning as a sensor. The RI of the external material serves as a significant external factor affecting the signal propagation in the microcavity sensor system. Consequently, the measurement of RI finds widespread application across diverse fields, such as environmental monitoring, biochemical sensing, and medicine [23–26]. The side-hole optical fibre (S-H OF) is a special fibre that serves as the foundation for many detection systems

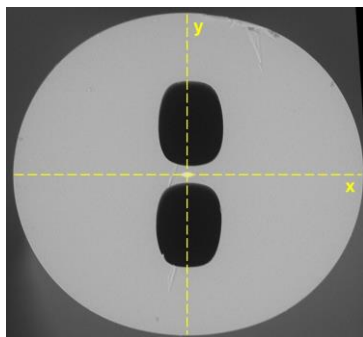
\*Corresponding author at: [rafal.kosturek@wat.edu.pl](mailto:rafal.kosturek@wat.edu.pl)

distinguished by its unique geometry [27, 28]. It is composed of an elliptical core and two air tunnels nearby. Conducting micromachining on such a fibre allows access to one of the air holes, enabling interaction with the propagating light by filling the manufactured microcavity with an external material [29, 30].

Microcavities fabricated on the surface of optical fibres exhibit resonant characteristics due to light interference within the cavity. When light enters the microcavity, it reflects multiple times between the cavity walls, creating standing waves at specific resonant wavelengths. The resonant condition is highly sensitive to changes in the external RI surrounding the microcavity [31, 32]. As the external RI increases, the effective RI within the cavity changes, which alters the resonance conditions [33]. The technological work presented in this article specifically focuses on creating an intensity sensor using cavity structures on S-H OF.

## 2. Techniques

Before initiating the laser micromachining of the cladding layer, the S-H OF was pre-positioned so that the shorter y-axis was vertical (Fig. 1).

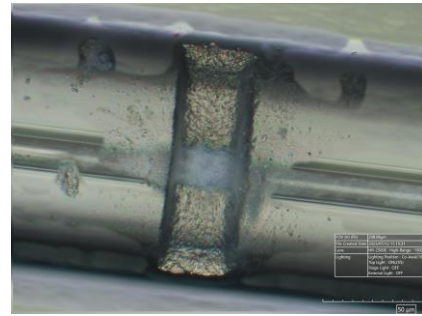


**Fig. 1.** Adopted coordinate system in the cross-section of the S-H OF.

The micromachining process was conducted in an ultra-precise multi-axis positioning system and femtosecond laser operating at 1030 nm wavelength. The laser provides pulses of a duration of 320 fs with a repetition rate of 1 kHz and a single pulse energy of 6.5  $\mu$ J. The S-H OF is fixed in holders and precisely positioned under the microscope objective. Specialized software for controlling the laser pulse triggering and the movement of the multi-axis positioning system allows for arbitrary material removal with a sub-micrometer precision. The spot size is limited by the numerical aperture (NA) of the objective used in the process. With a wavelength of 1031 nm and NA = 0.4, the spot size in the focal plane is estimated to be around 1.3  $\mu$ m in diameter. The effective area of the ablation of the material from the fibre is larger and close to 3  $\mu$ m. The microcavity is created by the line-by-line removal of a thin layer of glass material. The process is repeated layer-by-layer until the required depth of the microcavity is reached.

The final result of the micromachining was the creation of a microcavity providing access to one of the air tunnels with the following parameters: depth  $40 \pm 0.5$   $\mu$ m, length  $35 \pm 0.5$   $\mu$ m (first combination), length  $60 \pm 0.5$   $\mu$ m (second combination). The surface of the S-H OF after micro-

machining meets the desired dimensions and exhibits slight roughness (estimated  $\sim 3$   $\mu$ m). Courtesy of Technolutions, sample images were captured using a HIROX-HRX-01 system. An example photo is presented in the illustration below (Fig. 2).



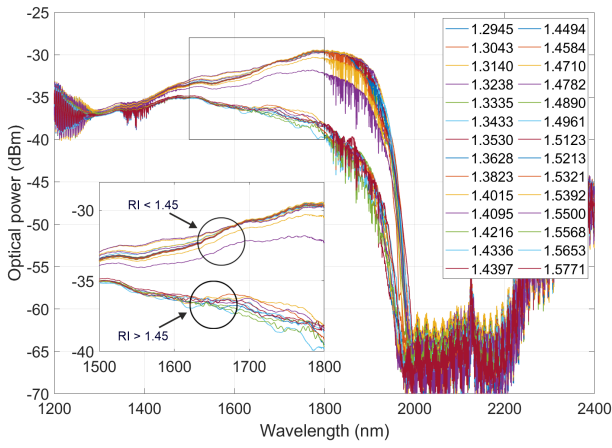
**Fig. 2.** Picture of a microcavity with a length of 35  $\mu$ m manufactured on the S-H OF.

Micromachined S-H OF was spliced with a standard SMF fibre at both ends with the use of a VYTRAN FFS-2000WS fusion splicer. The spliced SMF-S-H OF structure was linked with FC/PC connectors to a supercontinuum source at one end and an optical signal analyzer at the other. In the next step, an immersion liquid was applied to the microcavity with RI values ranging from 1.3 to 1.57 in increments of 0.02. Direct observation of the cavity under a microscope confirms that the capillary forces and viscosity of the oils used in the experiment enable a very effective filling. After applying the liquid to the microcavity, the influence of its application on the spectral characteristics was examined, followed by cleaning it with 99.8% isopropanol. Preceding the application of the immersion liquid by the process of splicing the S-H OF with the SMF generates pressure in the air tunnel, which prevents the liquid from entering the holes. The impact of the subsequent RI on transmission was studied after restoring the optical power to the reference level. The optical power losses for each immersive liquid were examined for the 1200–2400 nm wavelength range. The research was conducted for microcavities of 35  $\mu$ m and 60  $\mu$ m widths.

## 3. Results

The Fiber Optics Technology Laboratory at Maria Curie-Skłodowska University in Lublin, Poland, manufactured the S-H OF used in research. The produced fibre featured an elliptical core of  $1 \times 2 \pm 0.1$   $\mu$ m and air holes with dimensions of  $20 \times 35 \pm 0.1$   $\mu$ m.

In the first step, the effect of immersing the liquid on the spectral characteristics of the 35  $\mu$ m microcavity was examined. In the studies on the sensitivity of the external RI, immersion liquids in the 1.3–1.57 RIU (refractive index unit) range were used. It should be noted that RI is unitless (as the ratio of the speed of light in a vacuum to the speed of light in a particular medium), however, RIU is commonly used for describing RI sensors sensitivity, i.e., dB/RIU [29]. The optical power characteristics were plotted for a given wavelength. The chart presented is an average of the three-measurement series for each RI value (Fig. 3). All measurements were carried out at room temperature.



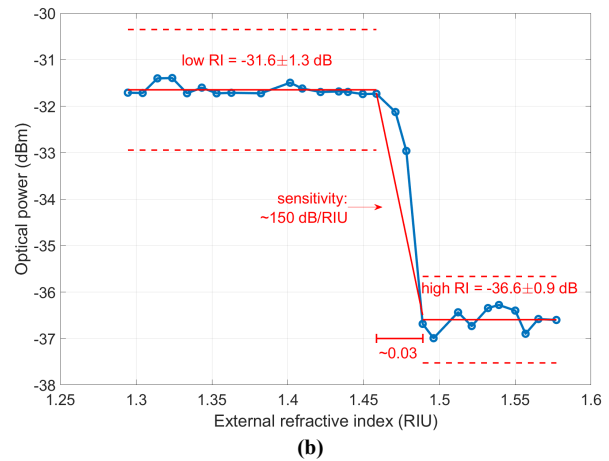
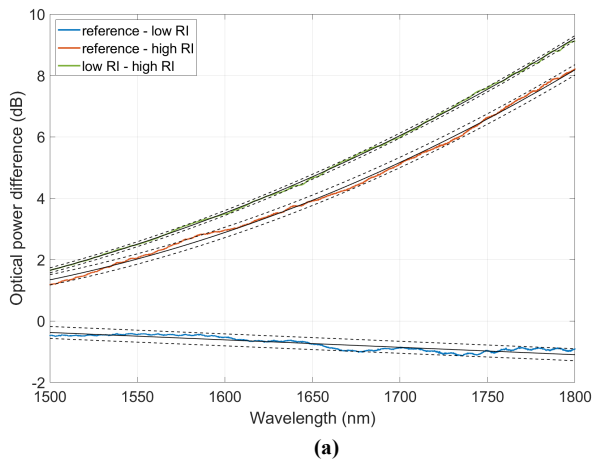
**Fig. 3.** Optical power dependence for applied immersion liquids in a wide spectrum range (1200–2400 nm).

The results indicate a slight influence of immersion liquids with the RI ranges of 1.3–1.45 and 1.49–1.57 on the transmission spectrum. For both ranges, the results show a constant level of transmission. In the next step of analysis for the 35  $\mu\text{m}$  microcavity, the 1500–1800 nm range was used. The selection of the wavelength range is related to the optical power characteristics of the microcavity, particularly concerning the depth of light penetration and the associated

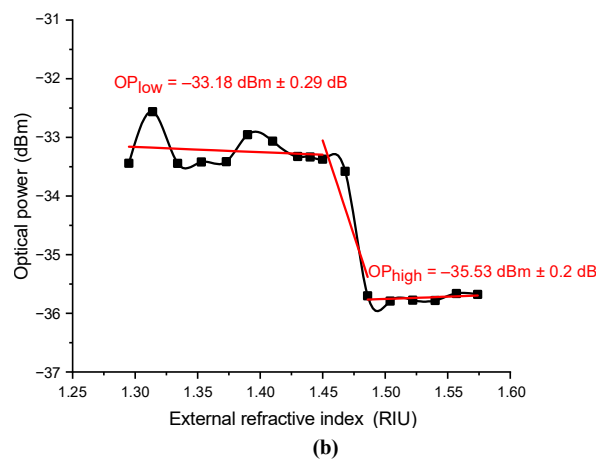
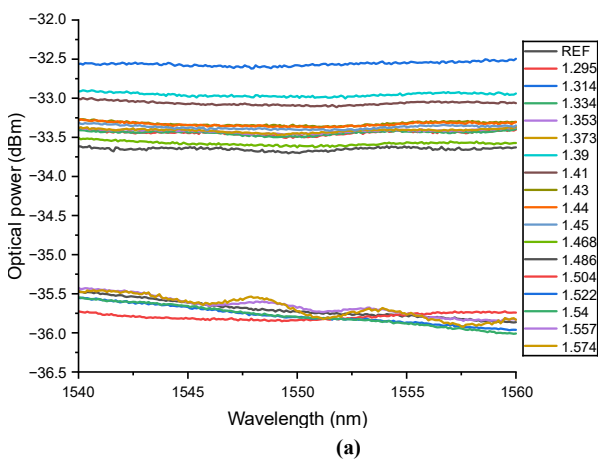
losses. The most distinctive range of the external RI is 1.46–1.49, where the highest dependence of the optical power level on the deposited immersion liquid is observed, with the sensitivity ( $S_{RI}$ ), described by the value of the slope coefficient for the obtained curve [34–36], approximately equal to 150 dB/RIU. There is a noticeable transition in optical power losses from an average level of  $-31.6 \text{ dB} \pm 1.3 \text{ dB}$  for RIs below 1.46 to  $-36.6 \text{ dB} \pm 0.9 \text{ dB}$  for RIs above 1.46. The following charts depict the difference in the averaged optical power spectra [Fig. 4(a)] and the averaged optical power values in the 1500–1800 nm range [Fig. 4(b)].

Further analysis focused on the narrower wavelength range of 1540–1560 nm due to the highest stability of the conducted measurements. Below are the results for the second sample with similar geometric parameters (Fig. 5).

The obtained spectral characteristics for applied immersion liquids in the range of 1.3–1.57 show disrupted optical power levels in the RI range of 1.3–1.46, with the highest power fluctuations observed at  $-32.5 \text{ dBm}$  to  $-33.7 \text{ dBm}$  for an RI of 1.32. The transmitted power for the RI range of 1.46–1.57 exhibited a constant optical power level. Once again, as with the previous sample, there is a noticeable power drop after exceeding an RI value of 1.46. The next research stage was conducted for a microcavity with a length of 60  $\mu\text{m}$ , using RIs in the range of



**Fig. 4.** (a) Difference in averaged optical power spectra and (b) averaged optical power values in the range of 1500–1800 nm.



**Fig. 5.** (a) Optical power dependence for applied immersion liquids in the narrow spectrum range of 1540–1560 nm. (b) Averaged optical power values in the range of 1540–1560 nm.

1.3–1.557. In the range from 1.3 to 1.46, no noticeable changes were observed in the spectral characteristics. The obtained results reveal characteristic wavelength dips for RIs above 1.47. To thoroughly investigate this phenomenon, studies were conducted on the influence of propagation direction on the obtained spectral characteristics. Below are the sample results of averaged optical power levels for RIs of 1.504 and 1.522 in the wavelength range of 1200–2000 nm (Fig. 6).

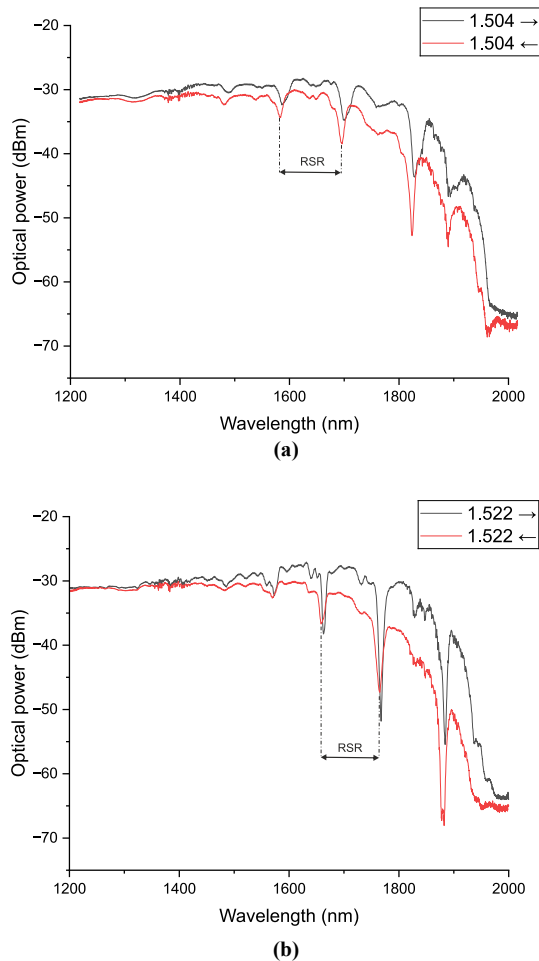


Fig. 6. The obtained spectral characteristics for both directions of light input for the immersion liquid with an RI: (a) 1.504, (b) 1.522.

The above results for both directions of light input into the fibre show dips for the same wavelengths. The differences in the transmitted power level for both directions most likely result from variations in the optical loss values of the splices. This article studies the distances between the wavelength dips described as the resonance spectral range (RSR). The spectral characteristics were examined for the average RSR depending on the RI value (Fig. 7).

An approximation of the obtained results indicated a decreasing RSR value with an increase in the RI of the applied immersion liquid. The sensitivity  $S_{RI}$  of the tested sensor system can be estimated from Fig. 7 at  $\sim 2621$  nm/RIU. The RSR value for an immersion liquid with an RI of 1.504 slightly disrupts the linear dependence of RSR on external RI. It is worth noting the slight change in the RSR values between RIs 1.504 and 1.522, where for 1.504, the RSR = 113 nm, while for 1.522, the RSR = 102 nm.

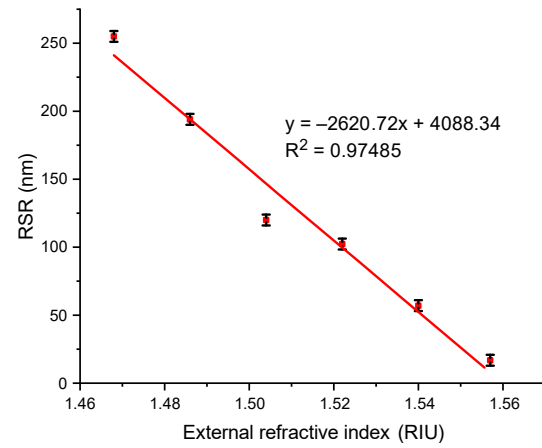


Fig. 7. The obtained RSR values of RIs ranging from 1.468 to 1.557.

The greatest change in RSR value occurred between immersion liquids with RIs of 1.486 and 1.504, where the difference in RSR = 81 nm.

Changes in RSR values with variations in the external RI are caused by changes in the resonance conditions. When the external RI changes, the phase-matching conditions for the light waves reflecting inside the cavity are modified. This shift changes the specific wavelengths that constructively interfere to form standing waves, resulting in different wavelength dips.

Table 1 compares the external refractive index sensitivity ( $S_{RI}$ ) of the sensor obtained in this work with the sensitivity of sensors from other literature reports. The authors included the 60  $\mu\text{m}$  microcavity in the comparison due to its higher sensitivity than the 35  $\mu\text{m}$  microcavity. The microcavity fabricated in this work exhibits a relatively high sensitivity but only for the tested range of RIs (1.464–1.557).

Table 1. External RI sensitivity of a microcavity-based sensor for different geometries and manufacturing technology.

Manufacturing technology	Microcavity type	$S_{RI}$ [nm/RIU] (RI range)	Ref.
Side-polishing	D-shape	$\sim 4122$ (1.333–1.398)	[34]
Fs laser	three-cascaded microchannels	$\sim 2406$ (1.33–1.38)	[35]
Polishing	fibre tip cavity	$\sim 1941$ (1.332–1.342)	[36]
Fs laser	D-shape S-H OF	$\sim 2621$ (1.468–1.557)	this work

The high sensitivity of the presented sensor structure, in the range of 1.464–1.557, paves the way for further research into its chemical and biological applications.

#### 4. Conclusions

In this study, the detection of the external RI depending on the geometry of a side-hole optical fibre microcavity was investigated. For a microcavity length of 35  $\mu\text{m}$ , the preliminary results obtained indicate no dependence of



transmission spectra on the external RI in two ranges of 1.30–1.45 and 1.49–1.57. Two constants levels of optical power can be distinguished, except for fluctuations in one of the samples after applying an immersion liquid with an RI of 1.32. A high dependence on the optical power level is visible in a very narrow range of RI changes (approximately 0.03), with a sensitivity of around 150 dB/RIU. This is linked to the fact that if the external RI is higher than the RI of the fibre, there is a leakage of cladding modes beyond its area. For the microcavity with a cut length of approximately 60  $\mu\text{m}$ , characteristic wavelength dips are observed, suggesting the presence of resonant modes inside the cavity. The decrease in RSR values with increasing external RI suggests a linear relationship between the two parameters. Based on the gathered results, it is possible to fabricate a sensor for an external RI by performing laser micromachining of the S-H OF cladding with access to one of the air holes. The results for the microcavity with a length of approximately 35  $\mu\text{m}$  suggest the possibility of RI detection based on the transmitted power level, although for the narrow range of 1.46–1.49. The analysis of results for the 60  $\mu\text{m}$  microcavity suggests a sensing potential based on RSR readings for RI (1.464–1.557). This microcavity geometry demonstrated a sensitivity of approximately  $\sim 2621$  nm/RIU. Based on the obtained results, it can be concluded that the sensor reported in the authors' study can be used for further research focused specifically on the detection of chemical and biological factors. Since the study used a supercontinuum light source, which is unpolarized, polarization control of the input beam was not conducted. The research results, supplemented by such an analysis, will be the subject of future studies.

### Authors' statement

Research concept and design, R.K. and M.D.; collection and/or assembly of data, R.K. and M.D.; data analysis and interpretation, R.K. and M.D.; writing the article, R.K., T.O., and M.Z.; critical revision of the article, L.R.J. and M.D.; final approval of the article, L.R.J.

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